Postural Function of the Diaphragm in Persons With and Without Chronic Low Back Pain

Despite the high prevalence of low back pain in the population, options regarding effective treatment strategies are still limited, possibly due to the lack of knowledge of the underlying mechanisms. Trunk stabilization and postural trunk control may play an important role in the etiology of low back pain. In turn, the function of the diaphragm may affect how the trunk is stabilized, especially during postural activity. Various studies have shown that the pelvic girdle and lumbar spine are reflexively stabilized and braced prior to the initiation of extremity movements. The central nervous system must be able to anticipate movement and stabilize the entire core musculature automatically to provide a stable base from which the muscles performing the movement can pull.

Trunk bracing maintains all spinal segments in a biomechanically neutral position during the course of any movement. Segmental movement (eg, hip joint movement) is therefore related to the synergistic activity of the spinal extensors and all the muscles modulating intra-abdominal pressure (ie, abdominal muscles, the diaphragm, and the pelvic floor). The diaphragm is the muscle that contributes the intra-abdominal pressure modulation and plays an important role in spinal stability.

Insufficient function and poor coordination of postural, or stabilizing, muscles are considered to be important etiological factors in spinal disorders associated with low back pain, such as deformational spondylolaurthesis (with or without spinal disc herniation), spinal disc protrusion, and/or spondylolisthesis. However, a study designed specifically to test the dynamics of the diaphragm in chronic spinal disorders is lacking. We aimed specifically to test the dynamics of the diaphragm in chronic spinal disorders. However, a study designed specifically to test the dynamics of the diaphragm in chronic spinal disorders is lacking.

### STUDY DESIGN
A case-control study.

### OBJECTIVES
To examine the function of the diaphragm during postural limb activities in patients with chronic low back pain and healthy controls.

### BACKGROUND
Abnormal stabilizing function of the diaphragm may be an etiological factor in spinal disorders. However, a study designed specifically to test the dynamics of the diaphragm in chronic spinal disorders is lacking.

### METHODS
Eighteen patients with chronic low back pain due to chronic overloadng, as ascertained via clinical assessment and magnetic resonance imaging, and 29 healthy subjects were examined. Both groups presented with normal pulmonary function test results. A dynamic magnetic resonance imaging system and specialized spirometric readings were used with subjects in the supine position. Measurements during tidal breathing (TB) and isometric flexion of the upper and lower extremities against external resistance with TB were performed. Standard pulmonary function tests, including respiratory muscle drive (P<sub>1,max</sub> and PE<sub>1,max</sub>), were also assessed.

### RESULTS
Using multivariate analysis of covariance, smaller diaphragm excursions and higher diaphragm position were found in the patient group (P<0.05) during the upper extremity TB and lower extremity TB conditions. Maximum changes were found in costal and middle points of the diaphragm. A 1-way analysis of covariance showed a steeper slope in the middle-posterior diaphragm in the patient group both in the upper extremity TB and lower extremity TB conditions (P<0.05).

### CONCLUSION
Patients with chronic low back pain appear to have both abnormal position and a steeper slope of the diaphragm, which may contribute to the etiology of the disorder.

### KEY WORDS
dynamic magnetic resonance imaging, lung function, spinal disorders, stabilizing function, thorax

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to examine diaphragm excursions and inspiratory/expiratory positions during normal tidal breathing (TB) and during postural tasks in patients with chronic low back pain and healthy volunteers. We hypothesized that the diaphragm excursions would be reduced in the patient group and that the inspiratory and expiratory positions of the diaphragm during postural tasks would be more cranial, reflecting abnormal diaphragm function. In addition, we expected that the recruitment manner of diaphragm sections during inspiration would show an altered contraction pattern in the patient group compared to healthy controls, indicating abnormal coordination. We assessed diaphragm positions using dynamic magnetic resonance imaging (MRI), with synchronized respiratory assessment during normal TB and postural limb activities, and analyzed respiratory muscle drive (maximum inspiratory/expiratory occlusion pressures).

**METHODS**

**Participants**

Participants recruitment occurred in 2 phases. All participants were recruited at the University Hospital Motol in Prague, Czech Republic, by a single clinician (P.K.). In the first phase, a sample of 30 healthy participants was recruited as part of a previously published study of the stabilizing function of the diaphragm. One participant was excluded due to insufficient data required for the present study. In the second phase, available volunteers with chronic low back pain due to vertebrogenic disorders were assessed (n = 18).

The inclusion criteria of the patient group included (a) low back pain that was not due to a specific injury and that could be classified as chronic (lasting at least 6 months), (b) a lack of systemic disease that would contribute to low back pain or morphological changes, and (c) observation of morphological changes of chronic character in the lumbar spine due to chronic overloading (morphology of the spinal disorder determined by MRI). Specifically, 7 patients were diagnosed with spondylosis and spinal stenosis, 2 patients with spondylosis and spondylolisthesis, 5 patients with spondylosis and disk hernia, and 4 patients with failed back surgery syndrome (patients operated for advanced spondylosis, spinal stenosis, and disk hernia not due to an injury). None of these conditions were a result of a spine or pelvic traumatic injury, or a chronic systemic or respiratory disease. Rather, we determined via clinical and MRI assessment that the morphological findings were consistent with abnormal stress to the structural elements of the lumbar spine. None of the patients suffered from chronic respiratory disease or such symptoms at the time of the study. Finally, participants who underwent a surgery for low back pain, listing injury as the primary cause, and patients in whom injury or a cause other than overuse or misuse contributed substantially to morphological changes in the lumbar spine were excluded.

The healthy participants (controls) included 4 males (14%) and 25 females (86%), with a mean ± SD age of 29 ± 7 years and body mass index (BMI) of 22.3 ± 2.5 kg/m² (height, 168 ± 8 cm; weight, 64 ± 8 kg). The 18 patients with chronic low back pain included 11 males (61%) and 7 females (39%), with a mean age ± SD of 48.6 ± 13 years and BMI of 26.8 ± 3.6 kg/m² (height, 177 ± 11 cm; weight, 84 ± 16 kg).

**Procedures**

This study was approved by The Institutional Ethical Committee. All participants underwent an in-person interview to ensure that they met the inclusion criteria of the study. All testing procedures were thoroughly explained to the participants with a detailed description of the dynamic MRI and spirometry assessments. All subjects reported that they understood the test procedures and gave their informed consent. Subjects were also instructed to fast at least 4 hours before each assessment procedure.

Participants were evaluated by dynamic MRI, with simultaneous respiratory recordings. Diaphragm activity, measured by excursion of the diaphragm, was evaluated by dynamic MRI, with subjects in the supine position, their heads supported 5 cm above the MRI plinth. Volumetric changes during the breathing cycle were recorded with a specially designed spirometer and specialized computer software. The subjects wore nose clips to prevent any air exchange through the nostrils. A mouthpiece connected to a pneumotachograph was placed in the subject’s mouth, and the subjects were allowed to practice normal breathing through the mouthpiece. After the subjects were trained in normal breathing with the mouthpiece for 2 minutes, measurements were taken during TB at rest and again with isometric limb contractions of the upper and lower extremities.

To ensure consistency during the testing procedures, the same physical therapist (P.K.) performed all assessments. Data collection time was 20 seconds in each condition per subject to record standard MRI measurements together with the respiratory readings.

Diaphragm activity was assessed under the following conditions (FIGURE 1). In all conditions, the subject was in the supine position with arms and legs relaxed along the torso. The subject was instructed to breathe normally throughout the assessment. The measurements of diaphragm movement and respiratory readings were recorded throughout the 20-second data collection period.

**Tidal Breathing** After the initial synchronization between respiratory and MRI recordings, simultaneous synchronized respiratory and MRI recordings were taken.

**Isometric Flexion of Upper Extremity (UE)** The clinician placed his hands on the dorsal surface of the subject’s forearms, which were at rest. The subject was then instructed to keep the elbows straight and flex both shoulders, attempting to lift the arms against the clinician’s resistance, maintaining an isometric con-
traction (FIGURE 1C). The muscle power generated by the subject corresponded to a grade 4 manual muscle test.25

**Isometric Flexion of Lower Extremity (LE)** The clinician placed his hands on the anterior surface of the subject’s thighs while the subject remained at rest. The subject was then instructed to perform bilateral hip flexion against the clinician’s resistance, maintaining an isometric contraction (FIGURE 1B). The muscle power generated by the subject corresponded to a grade 4 manual muscle test.25

All subjects were able to achieve grade 4 force, without substantial pain. As the clarity of MRI images is negated by involuntary and/or excessive movement, the inevitable movement caused by substantial pain during the performed postural activities would have resulted in images that could not be interpreted.

**MRI Assessments**

MRI scans and MRI analysis of diaphragm movement were performed using the approach described previously.27

The diaphragm was imaged in the sagittal plane with the subject in supine, using a body coil. The imaging plane was placed sagittally in the axial topogram directed paravertebrally to the right, midway between the center of the vertebral body and the edge of the thoracic wall. Slice thickness was 32 mm. Sequence duration was 20 seconds. Each subject had 3 markers (10-mL syringes of water) affixed to the skin surface and placed at (1) the midclavicular line, level of the jugular opening, (2) the inferior ventral costal margin, midclavicular line, and (3) the thoracolumbar junction in the dorsal axillary line.

The MRI image files were converted to Analyze format with MIRcro software. In each 20-second sequence, the baseline position of the diaphragm was determined for TB and postural activity conditions. The most caudal baseline position of the diaphragm was subtracted from the position of the other images in the sequence to determine the position changes of the diaphragm throughout the 20-second collection period. FIGURES 2A and 2B provide examples of the crescent-shaped image of diaphragm excursion, contrasting the most caudal and cranial diaphragm positions during TB in a healthy control (FIGURE 2A) and a patient with chronic low back pain (FIGURE 2B).

The diaphragm excursion images were converted to binary images to calculate their area in pixels. The bottom edge of the diaphragm excursion represents the most caudal baseline diaphragm position during inspiration. The top edge of the diaphragm excursion represents the diaphragm in its most cranial position during expiration. Successive images with the next highest pixel count were analyzed in order as the excursion of the diaphragm changed during the breathing cycle.

The next analysis was completed on the subtracted maximal crescent area of each image, where the horizontal, anterior/posterior alignment (perpendicular to the body axis), used as baseline, was represented in the front (point A in FIGURE 2C) by the inferior ventral costal margin, midclavicular line, and in the back (point E in FIGURE 2C) by the thoracolumbar junction in the dorsal axillary line. Markers designating the baseline were placed on each subject’s body (the total anterior/posterior distance was linked with the dotted line from point A to point E). The total horizontal distance was divided into 6 equal sections, demarcating 5 equidistant points, with point C marking the midpoint of the line from points A to E. The image series were converted into a binary state with the baseline being represented as white and areas of diaphragm excursion as black pixels. The upper and lower edges of the diaphragm were determined as average change from the baseline at each of the 3 middle points (B, C, and D) across all breaths taken within the 20-second interval. The distance at each point from the horizontal baseline was calculated to determine the difference in inspiratory position compared to the expiratory position of the diaphragm in millimeters (B1-B2, C1-C2, and D1-D2) (FIGURE 2C).

**Synchronized Respiratory Measurements**

Synchronized respiratory recordings and their processing were performed using the approach described previously.27 Tidal volumes were recorded with
a spirometer (MasterScope Jaeger Version 4.67; Jaeger, VIASYS, Würzburg, Germany) by a specially designed pneumotachograph with a plastic isoresistive membrane. This device allowed safe and reliable respiratory recording while in a strong magnetic field. A specialized reading and recording BreathRecorder software (J. Volejník, Kurka-Jaeger Servis, Ltd, Czech Republic) was developed for the purposes of this study. The flow signal measured the airflow, which was then converted and digitally integrated to yield the measurement of volume using an analog-to-digital converter and saved on a hard disk. Prior to respiratory measurements, every subject was familiarized with the mouthpiece in a supine position for a 2-minute period, during which no recordings were performed. The recording system was calibrated to each subject using a 1-L calibration pump prior to data collection.

The respiratory data were processed using Software Grapher (J. Volejník, Kurka-Jaeger Servis, Ltd, Czech Republic). From the 20 seconds of recorded data in each condition, 4 to 7 respiratory cycles were used to calculate the tidal volume. **Synchronization of Respiratory Measurements and MRI Sequence** The respiratory measurements were synchronized at the beginning of the 20-second MRI sequence within the initial 200 to 300 milliseconds by an electronic marker imprinted simultaneously on both recordings. The individually marked respiratory recordings were converted to DICOM format and synchronized with the dynamic MRI sequence of diaphragm movement images. The synchronized progression of the trace volume-time respiratory curve and the corresponding diaphragm movement were monitored using RADinfo Scan View System software (Radiology Information Systems, Inc, Sterling, VA).

**Pulmonary Function Tests**
Standardized spirometric recordings of pulmonary function tests (PFTs) were performed on the same day for all subjects with a MasterScope Jaeger spirometer (Version 4.5; Jaeger, VIASYS, Würzburg, Germany), with a special module for the assessment of respiratory muscles (drive). This is a widely used method that has been described elsewhere. In brief, the patients were instructed to maintain maximum inspiratory and expiratory pressure for at least 1.5 seconds, so that the maximum pressure sustained for 1 second could be recorded. The measured airway opening pressure for both maximum static inspiratory (PI_{max}) and maximum static expiratory pressure (PE_{max}) indicates global respiratory muscle output. All subjects were properly instructed and coached by an experienced technician during all PFTs. Proper procedures for quality assurance, based on the criteria of the American Thoracic Society, were used for these measurements. The following spirometric parameters were measured: forced expiratory volume in 1 second (FEV_{1}), forced vital capacity (FVC), and FEV_{1}/FVC. Concomitantly, assessments of respiratory muscles were performed. The following parameters used for these measurements were PI_{max} and PE_{max}. Procedures and quality criteria of the American Thoracic Society were used for these measurements. The PFT results were compared to established reference values using a regression equation that included age, sex, and height, which correlated most strongly with the respective normative values, along with the published regression coefficients as predictors of the observed values. The results are presented as percentages of the predicted values. The standard deviation of the residual of the predicted values (ie, the difference between the observed and
predicted values) was used to assess normality of the PFT results.

Pulmonary function tests yielded a predicted mean \( \pm \) SD FEV\(_1\) of 105.4\% \( \pm \) 9.6\%, FVC of 109.7\% \( \pm \) 12.0\%, and FEV\(_1\)/FVC of 99.5\% \( \pm \) 8.3\% for the healthy controls, and FEV\(_1\) of 106.1\% \( \pm \) 14.2\%, FVC of 113.8\% \( \pm \) 16.0\%, and FEV\(_1\)/FVC of 95.3\% \( \pm \) 11.6\% for the patients with chronic low back pain. All observed values fell within 1 standard deviation of the residual of the predicted values, deeming them within the normal range.

**Statistical Analysis**

All analyses were performed using commercial software SPSS Version 15 (SPSS Inc, Chicago, IL). First, we used multivariate analyses of covariance (MANCOVAs) within the general linear model statistical framework\(^{27}\) to assess group differences in diaphragm function. The MANCOVA yields an overall (multivariate) main effect, commonly represented by the F value associated with Wilks’ lambda criterion. This statistic reflects the covariate-adjusted effect across the dependent variables, while taking into account the common variance shared by the dependent variables. The MANCOVA also yields covariate-adjusted main effects linked to the individual dependent variables, which we interpreted when the multivariate effect was statistically significant.

Group (patient group versus control group) served as the independent variable across the models. The dependent variables were diaphragm excursions at each point of measurement, estimated separately for the TB, upper extremity TB (UETB), and lower extremity TB (LETB) conditions. In subsequent analyses, we examined group differences in the individual inspiratory or expiratory diaphragm positions by entering as the dependent variables the 3 points of measurement on the diaphragm during the TB, UETB, or LETB conditions.

We also tested whether coordination of the individual sections of the diaphragm (the recruitment manner) would be reduced during inspiration in patients with chronic low back pain. We

### TABLE

**Inspiratory and Expiratory Positions of the Diaphragm (mm)**

<table>
<thead>
<tr>
<th></th>
<th>Controls</th>
<th></th>
<th>Cases</th>
<th></th>
<th>Mean Difference</th>
<th>95% CI</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Mean</td>
<td>SD*</td>
<td>Mean</td>
<td>SD*</td>
<td>Mean Difference</td>
<td>95% CI</td>
</tr>
<tr>
<td><strong>Tidal breathing, inspiration</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Point B</td>
<td>94.1</td>
<td>29.4</td>
<td>92.8</td>
<td>26.1</td>
<td>1.3</td>
<td>-15.3,18.0</td>
</tr>
<tr>
<td>Point C</td>
<td>94.8</td>
<td>30.9</td>
<td>92.9</td>
<td>29.3</td>
<td>1.9</td>
<td>-16.3,20.0</td>
</tr>
<tr>
<td>Point D</td>
<td>77.9</td>
<td>33.5</td>
<td>71.0</td>
<td>31.4</td>
<td>7.0</td>
<td>-12.6,26.5</td>
</tr>
<tr>
<td><strong>Tidal breathing, expiration</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Point B</td>
<td>119.1</td>
<td>23.4</td>
<td>115.6</td>
<td>23.3</td>
<td>3.5</td>
<td>-10.7,17.7</td>
</tr>
<tr>
<td>Point C</td>
<td>127.8</td>
<td>24.0</td>
<td>125.8</td>
<td>23.6</td>
<td>2.0</td>
<td>-12.5,16.4</td>
</tr>
<tr>
<td>Point D</td>
<td>118.2</td>
<td>24.3</td>
<td>112.8</td>
<td>23.8</td>
<td>5.4</td>
<td>-9.2,20.0</td>
</tr>
<tr>
<td><strong>Upper extremity resistance, inspiration</strong></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Point B</td>
<td>90.1</td>
<td>29.7</td>
<td>123.3</td>
<td>50.4</td>
<td>-33.1</td>
<td>-60.1,-6.1</td>
</tr>
<tr>
<td>Point C</td>
<td>88.3</td>
<td>31.3</td>
<td>121.3</td>
<td>52.8</td>
<td>-33.0</td>
<td>-61.3,-4.7</td>
</tr>
<tr>
<td>Point D</td>
<td>67.6</td>
<td>34.9</td>
<td>89.6</td>
<td>50.9</td>
<td>-22.0</td>
<td>-49.9,6.0</td>
</tr>
<tr>
<td><strong>Upper extremity resistance, expiration</strong></td>
<td></td>
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<td></td>
<td></td>
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</tr>
<tr>
<td>Point B</td>
<td>119.8</td>
<td>23.2</td>
<td>126.5</td>
<td>24.5</td>
<td>-6.7</td>
<td>-21.3,7.9</td>
</tr>
<tr>
<td>Point C</td>
<td>127.6</td>
<td>23.8</td>
<td>139.2</td>
<td>27.2</td>
<td>-11.7</td>
<td>-27.5,4.2</td>
</tr>
<tr>
<td>Point D</td>
<td>116.2</td>
<td>25.1</td>
<td>130.8</td>
<td>34.8</td>
<td>-14.6</td>
<td>-33.9,4.7</td>
</tr>
<tr>
<td><strong>Lower extremity resistance, inspiration</strong></td>
<td></td>
<td></td>
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<td></td>
<td></td>
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</tr>
<tr>
<td>Point B</td>
<td>85.7</td>
<td>32.6</td>
<td>120.1</td>
<td>46.1</td>
<td>-34.3</td>
<td>-57.5,-11.2</td>
</tr>
<tr>
<td>Point C</td>
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<td>34.4</td>
<td>115.7</td>
<td>47.2</td>
<td>-34.0</td>
<td>-60.2,-7.7</td>
</tr>
<tr>
<td>Point D</td>
<td>59.7</td>
<td>38.2</td>
<td>82.8</td>
<td>46.8</td>
<td>-23.1</td>
<td>-49.9,2.1</td>
</tr>
<tr>
<td><strong>Lower extremity resistance, expiration</strong></td>
<td></td>
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<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Point B</td>
<td>116.5</td>
<td>25.4</td>
<td>125.2</td>
<td>25.3</td>
<td>-8.6</td>
<td>-24.0,6.7</td>
</tr>
<tr>
<td>Point C</td>
<td>122.1</td>
<td>25.7</td>
<td>136.5</td>
<td>29.1</td>
<td>-14.5</td>
<td>-30.8,19</td>
</tr>
<tr>
<td>Point D</td>
<td>109.0</td>
<td>28.1</td>
<td>125.3</td>
<td>36.7</td>
<td>-16.3</td>
<td>-36.9,4.4</td>
</tr>
</tbody>
</table>

Abbreviations: CI, confidence interval.
*Standard deviation from the mean.
†Differences in means: lower and upper limits for the 95% CI around the difference in means; a result is significant when the CI does not cross zero.
‡Points B, C, and D refer to the anterior, middle, and posterior parts of the diaphragm, as illustrated in FIGURE 2.
calculated a slope of the middle-posterior diaphragm for each participant by subtracting values for the middle and posterior inspiratory positions and compared mean values between groups using a 1-way analysis of covariance (ANCOVA), in which the slope of the middle-posterior diaphragm was the dependent variable, group (patient versus control) was the independent variable, and age and gender were the covariates.

To test coordination between the diaphragm and other respiratory muscles, we calculated Pearson correlation coefficients for the relationship between MRI-derived total diaphragm excursion, specified as the sum of diaphragm excursion at points B, C, and D for each postural task (TB, UETB, and LETB), and the 2 indices of respiratory muscle drive (PL_{max} and PE_{max}) separately in the control and patient groups.

Statistical significance was assessed at a 2-tailed .05 level across all analyses.

RESULTS

The table presents the unadjusted means and standard deviations for diaphragm position during the 3 tasks. Figure 3 illustrates inspiratory and expiratory diaphragm positions during normal TB (Figure 3A), UETB (Figure 3B), and LETB (Figure 3C).

The groups differed in age, gender, and body mass index (BMI). In an independent t test, with equal variances not assumed, the patient group was on average older (t[24] = 6.04, P < .001) and had higher BMI (t[27] = 4.70, P < .001) than the control group. There were more women than men in the patient group (χ² = 11.40, P < .001). Subsequently, we also found that age and BMI were highly correlated (r = .75, P < .001) and, in a 1-way analysis of covariance, BMI was not statistically different in the patient group compared to the control group when age was used as a covariate (F₁,₄₅ = 1.07, P = .31), indicating that the higher BMI in the patient group was attributable to the higher age in this group. To use a parsimonious model more amenable to the relatively small sample size, only age and gender were used as covariates in the MANCOVAs.

Diaphragm Excursions and Inspiratory/Expiratory Diaphragm Positions During TB

During TB without postural movement, the MANCOVAs yielded no significant multivariate effects for the differences between the patient and control groups in diaphragm excursions, as well as diaphragm inspiratory and expiratory positions (P > .05) (Figure 3A).

Diaphragm Excursions and Inspiratory/Expiratory Diaphragm Positions During Postural Activities

Differences between the patient and control groups emerged when postural tasks were applied during TB (Figures 3B and 3C). For diaphragm excursions, the MANCOVA-based multivariate effects for group were significant in both the UETB (F₁,₄₁ = 3.69, P = .020) and the LETB (F₁,₄₁ = 4.76, P = .006) conditions, indicating that diaphragm excursions were significantly smaller in the patient group compared to the control group under both conditions. In the UETB condition, the significant overall effect for group was attributable primarily to the group differences at point B (P = .016), whereas the differences at points C (P = .059) and D (P = .001) were not significant. In the LETB condition, the smaller diaphragm excursion in the patient group existed at points B (P < .001), C (P < .001), and D (P = .023).

We then assessed group differences in inspiratory and expiratory diaphragm positions individually. During the UETB condition, the multivariate main effect for group across the 3 points of measurement (B, C, and D) was significant during inspiration (F₁,₄₁ = 4.11, P = .012), indicating a higher (more cranial) position of the diaphragm in the patient group. This effect could not be attributed to any single point on the diaphragm (P > .30), although the group differences in diaphragm position appeared more pronounced at points B and C (Figure 3B). The multivariate main effect for group was not significant during expiration (P = .336).

During the LETB condition, the multivariate main effect for group was again significant during inspiration (F₁,₄₁ = 3.49, P = .024), with the diaphragm positioned higher in the patient group than the control group. As in the UETB condition, no single point represented this difference in diaphragm inspiratory position, with the group difference slightly larger at points B (P = .132) and C (P = .141) than D (P = .361). The multivariate main effect for group during expiration...
was not significant \((P = .40)\), although a post hoc analysis indicated that this effect was significant \((P = .022)\) when age and gender were not controlled.

The Recruitment Manner of the Diaphragm
In this step, we examined the hypothesis that diaphragm contraction during inspiration occurs more unevenly in the middle-posterior portion in the patient group. Given previous evidence and the angle variation illustrated in FIGURE 3, we tested whether poor coordination in the patient group was represented specifically by altered diaphragm contraction in the middle-posterior (crural) portion of the diaphragm, denoted as points C and D. The unadjusted means on which this analysis was based are presented in the TABLE. In an analysis of covariance examining group differences in the slope of the middle-posterior diaphragm controlling for age and gender, the main effect for group was not significant during the TB condition \((P > .05)\). However, there was a significant main effect for group during both the UETB (\(F_{1,43} = 10.07, P = .003\)) and the LETB (\(F_{1,43} = 5.49, P = .024\)) conditions, indicating that the contraction of the diaphragm followed a substantially steeper recruitment pattern in the patient group relative to the control group. For better illustration of this situation, FIGURE 4 shows the slope of the middle-posterior diaphragm during inspiration in the UETB condition.

Total Diaphragm Excursion and Respiratory Muscle Drive
No significant correlations emerged between total diaphragm excursion and \(P_{E_{\text{max}}}\) or between diaphragm excursion and \(P_{I_{\text{max}}}\) in the TB or UETB condition. However, in the LETB condition, positive correlation between diaphragm excursion and \(P_{I_{\text{max}}}\) was found in the patient group \((r = .50, P = .035)\) but not in the control group \((r = -.021, P = .916)\). These 2 correlations are illustrated in FIGURE 5. Fisher \(r\)-to-\(z\) transformation indicated that the difference between the 2 coefficients approached statistical significance \((P = .078)\).

DISCUSSION

We studied differences in diaphragmatic activity during TB with and without postural activities in a group of patients with chronic low back pain compared to healthy volunteers. We found that diaphragm excursions or inspiratory/expiratory positions did not vary across patients and controls during TB without postural tasks. However, reduced diaphragm movement emerged when isometric flexion against resistance of the upper or lower extremity was applied, pointing to the importance of postural tasks in the expression of abnormal diaphragm function. The results provide additional evidence for altered breathing patterns during strenuous and nonstrenuous activity in individuals with low back pain.24,30 The findings may support the notion that the strategies utilized by the central nervous system to control core stability are altered in the presence of painful syndromes.14

Perhaps the most clinically important finding of this study concerns the abnormal coordination of the diaphragm in the patient group during inspiration with postural tasks. This impairment was demonstrated by reduced movement of the diaphragm in the anterior and middle portion, while the posterior (crural) part moved in the same manner as in the control group. This pattern of diaphragmatic recruitment resulted in a steeper angle in the middle-posterior part of the diaphragm (FIGURE 4), which may exacerbate the symptomology of chronic
low back pain by increasing the anterior shear forces on the ventral region of the spinal column.

Although the role of the ligamentous and muscular system to stabilize the low back and decrease the shear forces during loading has been studied extensively, not much attention has been paid to the coordination across individual sections of the diaphragm. Additionally, while radiological evaluation or visualization of the diaphragm is routinely performed in clinical practice, to our knowledge, no research to date has been conducted in which diaphragm dynamics would be visualized in relation to postural tasks and low back pain. In the control group, normal diaphragmatic contraction performed during inspiration was characterized by a symmetric recruitment of all diaphragmatic parts, that is, points B, C, and D. This motion is directed downward toward the abdominal cavity. The physiologically domed (convex) contour of the diaphragm at the end of expiration becomes less domed, and thus the contour is more symmetrical at the end of inspiration.

By contrast, although the patient group demonstrated normal recruitment of the crural portion of the diaphragm, movement in the anterior and medial portions was limited in both postural tasks. Poor coordination of particular diaphragmatic parts in the patients (points B and C) resulted in an asymmetric diaphragmatic activation during inspiration, as demonstrated by a steeper slope of the crural part of the diaphragm. Evidently, limited motion of the costal part may result in a more domed inspiratory diaphragmatic position. Contraction of the diaphragm has been found to modulate intra-abdominal pressure and contribute to trunk stability. Although we did not measure intra-abdominal pressure directly, we suspect that in the patient group, abnormal position and recruitment of the diaphragm resulted in subsequent reduced intra-abdominal pressure conducive to low back pain. These findings are consistent with the hypothesis that abnormal postural activation of the diaphragm may serve as 1 underlying mechanism of chronic low back pain.

Finally, during LE flexion, total diaphragm excursions and maximum inspiratory pressure (PI max) in healthy controls (A) and patients with chronic low back pain (B).
sarily be reduced in the patient group. Previous research suggests that inhaled lung volume may even be greater in patients with low back pain, although this research did not include any measurement of diaphragm movement. Finally, we found pulmonary function within a normal range for both groups, further suggesting that compensation for the limited diaphragm movement might have occurred. Taken together, we speculate that an altered mode of activation, indicative of poor activation of the diaphragm during TB with postural tasks and more consistent activation of other respiratory muscles, may be typical in patients with chronic low back pain.

In healthy subjects, the diaphragm is able to perform the dual task (trunk stability and respiration) when trunk stability is challenged. Generally, during any body movement, with activation of the extremities during weight-bearing or weight-lifting activities and transitional movements, there is simultaneous spinal bracing and transdiaphragmatic pressure elevation. Intra-abdominal pressure increases, with a simultaneous decrease of intrapleural pressure, during a contraction of both the posterior (crural) and anterior (costal) portions of the diaphragm. This coordination may be compromised in patients with chronic low back pain.

Stabilizing postural activation of the diaphragm has been reported during, for example, weight lifting and isometric activation of the extremities. Similarly, higher inspiratory pressures and hypertrophic changes in the diaphragm have been demonstrated during exercise. It can be assumed that, in cases of postural instability, the insufficient stabilizers must be compensated by other muscles. A significant decrease in strength of trunk muscles, especially the extensors, in patients with low back pain has been established, suggesting that strengthening exercises of the trunk muscles may be an optimal rehabilitation strategy.

One possibility is that the lack of postural diaphragmatic activation is substituted by excessive activation of the superficial lumbar paraspinal muscles, which may lead to hypertrophy and, eventually, result in lumbar hyperlordosis and/or anterior pelvic tilt. Future research should study this mechanism as possibly contributing to or even underlying the etiology of low back pain symptoms. Furthermore, long-lasting effects and pain alleviation may be aided by achieving balanced agonist-antagonist postural activation (that is, balanced activation across the sections of the diaphragm, pelvic floor, and the abdominal wall and extensors). Research is needed to investigate the possibility that working to correct the altered function of the diaphragm specifically may contribute to alleviating low back pain symptoms by improving spinal stability.

There are several limitations to this study. First, we used a convenience sample in which the patient and control groups differed in size and some demographic characteristics. Although we used statistical methods appropriate for unbalanced designs and controlled for these differences statistically, we cannot fully exclude the possibility that these differences had some influence on the results. Second, ideally, the entire rib cage, including the whole range of diaphragm excursions, should have been imaged. Only an isolated analysis of the diaphragm was performed, which focused on the diaphragm excursions, due to the limited size of the field of view. Although we have limited the diaphragm excursion measurements to 3 points, this is similar to studies conducted by other authors and can be considered sufficient for this type of study. In addition, the diaphragm excursions alone may not be sufficient to understand all mechanical actions of the rib cage and related musculature. For example, individual breathing patterns may be considered along with diaphragm excursions in future research. Third, although external pressure to generate grade 4 force was applied by the same clinician (P.K.) and standardized requirements of current MRI methodology were followed in order to reduce variation in diaphragm motion and function, force and direction were not formally assessed. Therefore, we cannot exclude the possibility that the resistance varied across the subjects.

Fourth, we did not assess the length or duration of low back pain in the patient group, only that the pain had lasted at least 6 months. Nor did we assess pain during postural tasks. However, all participants exhibited the ability to perform grade 4 force without substantial pain. Had pain been present during postural tasks, we could not have obtained readable MRI images. It could also be argued that the 4 patients who underwent a failed back surgery might have differed from the rest of the patient sample in their outcomes. Excluding these 4 patients, however, would not have substantially altered the results, although group differences in diaphragm excursion during lower and upper extremity postural tasks were somewhat (not substantially) greater, as were group differences in the correlation between total diaphragm excursion and respiratory muscle drive. Finally, poor postural function of the diaphragm may result in symptoms of low back pain and lead to chronic verterogenic dysfunction. However, considering all possibilities, we cannot exclude the reverse order of events. Low back pain symptoms may be indicative of an initial pathogenic insult resulting in secondary quantitative as well as qualitative adaptive changes in diaphragmatic function.

CONCLUSION

We found reduced diaphragm movement when isometric flexion against resistance of the upper or lower extremities was applied. The combined, more cranial position in the anterior and middle portions of the diaphragm and, particularly, the steeper slope between the middle and cranial portions of the diaphragm in patients with chronic low back pain may contribute to low back pain symptoms. However,
given that the results are based on cross-sectional analysis, we cannot exclude the possibility of reverse causation. Still, the results support the theory that patients with low back pain complaints present with compromised diaphragm function, which may play an important role in postural stability.

**KEY POINTS**

**FINDINGS:** We found reduced diaphragm movement in patients with chronic low back pain compared to healthy controls when isometric flexion against resistance of the upper or lower extremity was applied, mainly in the anterior and middle portions. This pattern of diaphragmatic recruitment resulted in a steeper angle in the middle-posterior part of the diaphragm and likely a greater strain during activity on the ventral region of the spinal column.

**IMPLICATIONS:** Abnormal postural activation of the diaphragm during the postural task of isometric resistance to the extremities may serve as 1 underlying mechanism of chronic low back pain.

**CAUTION:** Only an isolated analysis of the diaphragm excursion was performed, due to the limited field of view. In addition, the diaphragm excursion alone may not be sufficient to understand all mechanical actions of the rib cage and related musculature. We used a convenience sample in which the patient and control groups differed in size and certain demographic characteristics. Because our study was cross-sectional in nature, we cannot exclude the possibility that low back pain symptoms may be indicative of an initial pathogenic insult resulting in secondary quantitative as well as qualitative adaptive changes in diaphragmatic function.

**REFERENCES**


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